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Fabrication Of Taste Masked Tablets Via Fused Deposition Modeling 3D Printing Paired With Hot-Melt Extrusion Techniques

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FABRICATION OF TASTE MASKED TABLETS VIA FUSED DEPOSITION MODELING 3D PRINTING PAIRED WITH HOT-MELT EXTRUSION TECHNIQUES

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ABSTRACT

The objective of this work was to develop taste-masked donut-shaped tablet formulations utilizing fused deposition modeling three-dimensional (3D) printing paired with hot-melt extrusion (HME) techniques. Caffeine citrate (CC) was used as the model drug for its bitter taste, and a three-point bend test was performed to assess the printability of filaments. The stiffness constant was calculated to represent the printability by fitting the breaking distances and stress data into Hooke's law. Formulation F6 and F7 filaments exhibited the desired hardness with a "k" value of 48.30 ± 3.52 g/mm^3 and 45.47 ± 3.51 g/mm^3, respectively, and were successfully printed. The donut-shaped tablets were 3D printed with 10%, 50%, and 100% infill densities. *In vitro* dissolution studies were performed in simulated salivary fluid (pH 6.8, artificial saliva) to evaluate the taste masking efficiency of the printed donuts. In the first minute, the concentrations of CC observed in the dissolution media from all the printed donuts were less than the bitter threshold of CC (0.25 mg/mL). Formulation F7, which contained Eudragit® E PO copolymer, demonstrated better taste masking efficiency than formulation F6. Furthermore, both formulations F6 and F7 demonstrated immediate drug release profiles in gastric medium (10% infill, >80% release within 1 h). Taste-masked CC formulations were successfully developed with donut shapes, which will enhance appeal in pediatric populations, and increase compliance and patient acceptance of the dosage form.

DEDICATION

This work is dedicated to my parents Mr. Xuefeng Wang and Mrs. Bing Li for all their support, encouragement and affection all through these years.

ACKNOWLEDGMENTS

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TABLE OF CONTENTS

LIST OF TABLES

TABLE PAGE

LIST OF FIGURES

FIGURE PAGE

1. INTRODUCTION

Oral drug delivery is the most employed and convenient of all drug administration routes. A significant number of active pharmaceutical ingredients (APIs) used in oral drug delivery systems have a bitter taste [1]. The bitterness of oral drug delivery systems influences compliance and patient acceptance of dosage forms [2], especially in pediatric populations. The mechanisms of commonly used taste-masking techniques can be summarized as three aspects: a physical barrier, chemical or solubility modification of active pharmaceutical ingredients, and the formation of solid dispersions [3]. Various methods to mask the taste of bitter APIs are lipid barrier systems [4], cyclodextrin inclusion [5], film coatings [6], ion-exchange resins [3, 7], microspheres [8], solid lipid pellets [9], and microencapsulation [10].

Hot-melt extrusion has been employed as a novel manufacturing technique of various solid oral dosage forms in the last two decades. It was used in the production of immediate-release dosage tablets [11, 12], modified-release formulations including sustained release dosage forms [13-16], enteric release formulations [17], targeted release systems [18], chrono-modulated drug delivery systems [19], and novel taste-masked and abuse deterrence formulations [11]. Taste masking is achieved by modifying drug release from the polymer matrix to prevent bitter APIs from contacting the patient's taste buds [20]. HME is a continuous, solvent-free process, has a short processing time, and is easy to scale-up, and several polymer-carriers and other additives used during extrusion processing are generally known to be safe for consumption [21, 22]. HME for manufacturing taste-masking dosage forms is, therefore, a

robust, cost-effective technique and has great potential for industrial scale-up.

Three-dimensional (3D) printing is a layer-by-layer manufacturing technique that produces 3D real objects from computer-aided designs using plastic and metal materials and has been developed for design, construction, aerospace, engineering, arts, and medical implant fabrications and devices due to its controllability and feasibility [23, 24]. Furthermore, 3D printing is a novel technology in the pharmaceutical industry, providing an effective solution for individualized, complex, and customized production of oral drug delivery systems [25]. 3D printing technology combines digital design, manufacturing, and controls together, which is an accurate, timesaving, continuous process to meet individual patient needs. These 3D printing technologies can be divided into three major categories: printing-based inkjet systems, nozzle-based deposition systems, and laser-based writing systems [26]. Fused deposition modeling (FDM) is a nozzle-based deposition system that creates solid objects by successive deposition of strands of molten polymers layer by layer via the nozzle of a moving printhead [27, 28]. FDM has several significant advantages such as low-cost manufacturing, a compatible downstream to take advantages of thermotolerant pharmaceutical polymers and APIs through hot-melt extrusion (HME), and the ability to design and manufacture novel drug delivery systems [29-31].

Personalized medicine aims to provide patients with treatments tailored to their pathophysiology. This tailoring is achieved by coupling a patient's pharmacogenomics with information about their diet, environment, lifestyle, microbiome, and epigenetics [24]. Personalized medicine is a key factor for future improvement in disease treatment and is administered to individual patients [32]. FDM 3D printing could be applied as a fabrication tool within digital health for the remote manufacture and dispensation of personalized formulations having doses, shapes, and sizes that are optimized for the patient. The therapy and medication

adherence may be enhanced owing to the flexibility and autonomy of the treatment process provided by 3D printing [33]. However, there is a lack of tailor-made taste-masking techniques for the masking of the unpalatable tastes of several drugs [34, 35].

Compared with traditional pharmaceutical product manufacturing processes, the combination of HME and 3D printing technology has two advantages: (1) the ability to fabricate immediate-release tablets, modified-release tablets, and other novel drug delivery systems; (2) the capability to produce more complex structured dosages and personalized drug products. Moreover, the combination of these two technologies reduces the downstream process that traditional manufacturing techniques involve, including milling extrudates, granulation, sieving, compressing, and coating, and thus renders them more efficient and economical [36, 37]. HME was employed to develop CC feedstock filaments using HPC and EPO as matrix polymers. Eudragit® E PO, a cationic copolymer based on dimethylaminoethyl and neutral methacrylic esters, dissolves at pH < 5 and remains intact at neutral pH, which offers a potential application for taste masking [38].

Caffeine citrate, an odorless, bitter-tasting, Biopharmaceutics Classification System (BCS) class-I drug, was chosen as a model drug. It has a rapid dissolution rate in the oral cavity; thus, taste masking can be achieved by retarding the dissolution process using HME and 3D printing. The novelty of this investigation is to apply pair fused deposition modeling (FDM) 3D printing with HME technology to design and fabricate tailor-made taste-masked donut-shaped tablets to enhance patient compliance, especially in pediatric populations.

2. MATERIALS AND METHODS

2.1 MATERIALS

Caffeine citrate (CC) was purchased from Fisher Scientific (Pittsburgh, PA, USA). Klucel™ HPC, HF, and LF, and Benecel™ HPMC K4M were donated by Ashland Inc. (Covington, KY, USA). Eudragit® E PO was supplied by Evonik Industries (Essen, Germany). All other reagents were of analytical grade.

2.2 METHODS

2.2.1. FORMULATIONS

Initially, HPC LF, a commonly used polymer for 3D printing, was chosen to develop the formulations (Table 1). HPMC K4M was used to achieve desirable mechanical properties and printability of filaments, and Eudragit® E PO was added to improve the taste-masking ability of the 3D printed donut-shaped tablets.

Table 1. Compositions of the formulations.

Formulation	**Drug (w/w)**	**Polymer (w/w)**
F1	5%	95% HPC LF
F2	10%	90% HPC LF
F3	15%	85% HPC LF
F4	20%	60% HPC HF + 20% Eudragit EPO
F5	20%	60% HPC LF + 20% HPMC K4M

F6	15%	65% HPC LF + 20% HPMC K4M
F7	15%	60% HPC LF + 20% HPMC K4M + 5% Eudragit EPO

2.2.2. HOT-MELT EXTRUSION

The extruder (Thermo Fisher Scientific, Waltham, MA, USA) used in this study was a co-rotating, twin-screw extruder with 11 mm diameter screws, a length: diameter ratio of 40:1, and eight electrically heated zones. Physical mixtures of formulation ingredients were extruded at 155 °C and a screw speed of 50 rpm. A standard screw configuration with three mixing zones provided by Thermo Fischer and a 1.5 mm round die was used to extrude filaments for 3D printing. The filaments were cooled and straightened using a conveyor belt at the extruding speed before loading into the 3D printer. Polylactic acid (PLA) without drug load was used as a reference to test the stiffness constant.

2.2.3. DIFFERENTIAL SCANNING CALORIMETRY (DSC)

A DSC system (TA Instruments, New Castle, DE, USA) was used to study the crystallinity of the drug, the thermostability of the ingredients, and the nature of the drug in the filaments. Samples weighing 4-6 mg (pure ingredients and milled filaments) were sealed into aluminum pans and placed on the testing zone, then heated to the temperature range 25–250 °C at a rate of 20 °C/min. Nitrogen was used as the purge gas at a flow rate of 50 mL/min. The associated Pyris DSC software was used to analyze the data and the DSC thermograms.

2.2.4. FUSED DEPOSITION MODELING 3D PRINTING

Donut-shaped structures were designed online using Autodesk Tinkercad software (Tinkercad, Autodesk Inc, CA, USA) and saved as gcode files for printing. A commercial FDM 3D printer (Prusa i3 3D desktop printer, Prusa Research, Prague, Czech Republic) was used to print donut-shaped tablets, while printing operation software (CURA version 15.04; Ultimaker,

Geldermalsen, Netherlands) was used to adjust the printing parameters. Donut dimensions were as follows (donut shape, diameter: 10 mm, height: 5 mm, radius (the distance between the tablet center to the tube center): 3.5 mm, tube thickness: 3 mm, wall thickness: 0.2 mm) (Fig. 1). The printing temperature was 200 °C, while the bed temperature was 60 °C, and the tablets were printed at three different (10%, 50%, and 100%) infill densities at a speed of 60 mm/sec. The degradation temperature of CC is over 250 °C, and all the excipients were stable at the processing temperature [21, 36].

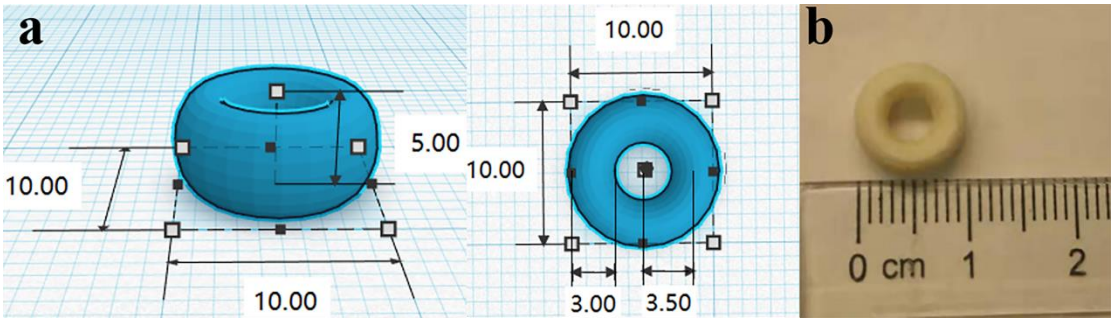

Figure 1. Dimensions of 3D printed tablets. (a) The view of tablet design (units: mm). (b) conventional photograph of the 3D-printed tablet.

2.2.5. THE REPKA-ZHANG TEST

In this study, Repka-Zhang methods were adopted to perform 3-point bend tests to evaluate the printability of filaments [36]. A TA-XT2 analyzer (Texture Technologies, Hamilton, MA, USA) and the TA-95N probe set were used for the flexibility and brittleness tests. The filament samples were cut into 6 cm rods, then placed on the sample holder (25 mm width gap). The blades moved at a speed of 10 mm/sec until reaching 20 mm below the tested sample. Testing for each single filament formulation was repeated 10 times. Polylactic Acid was used as a reference material to compare the differences between commercially available filaments and extruded filaments.

2.2.6. PREPARATION OF TABLETS BY DIRECT COMPRESSION

Conventional immediate-release tablets were formulated by direct compression for comparison of their drug release characteristics with 3D printed tablets. Based on the highest weights and drug loads of the 3DP tablets (100% infill), 220 mg of physical mixtures of each formulation was compressed into tablets using an 8 mm die at 50 bar. Formulation ingredients consisted of caffeine citrate (13.6%), croscarmellose sodium (8%), magnesium stearate (0.5%), and microcrystalline cellulose (77. 9%). A VK200 Vankel Varian tablet hardness tester (Agilent Technologies, Santa Clara, CA, USA) was used to test the hardness of the direct compression tablets.

2.2.7. FOURIER TRANSFORM INFRARED SPECTROSCOPY (FTIR)

An Agilent Cary 660 FTIR spectrophotometer (Agilent Technologies, Santa Clara, CA, USA) was used to investigate interactions between the API and polymers over a 600–4000 cm-1 range. The FTIR spectra of the API, polymers, and milled extrudates were recorded.

2.2.8. SCANNING ELECTRON MICROSCOPE (SEM)

A Hummer® 6.2 sputtering system (Anatech LTD, Springfield, VA, USA) was used to investigate the surface morphology of the filaments and the cross-sections of 10% infill, 50% infill, and 100% infill printed tablets. The SEM apparatus (JEOL JSM-5600) operating system was set at an accelerating voltage of 5.0 kV for imaging [39]. The magnification of 25X, 50X, 100X, and 200X was investigated to understand the morphology of printed tablets.

2.2.9. *IN VITRO* DISSOLUTION STUDIES

A United States Pharmacopeia (USP) dissolution apparatus I (Hanson SR8-plus™; Hanson Research, Chatsworth, CA, USA) was employed to perform the *in vitro* dissolution studies. Each experiment was assessed in triplicate, and the temperature was set at 37± 0.5℃.

Gastric drug release occurred in 900 mL of 0.1 N HCl, and the baskets rotation speed was 100 rpm. Samples were collected at 5, 10, 15, 30, 60, 90, and 120 min time point, diluted, and analyzed using a UV-Vis spectrophotometer at 273 nm. Further, *in vitro* drug release was assessed using 500 mL of artificial salivary media adjusted to pH 6.8 [40]. The drug release was analyzed at 10 sec intervals for 10 min using Pion® dissolution apparatus equipped with a dynamic UV-Vis detector system (Rainbow Dissolution Monitor, Pion Inc., Billerica, MA, USA) at 273 nm. The basket rotation speed was set to 100 rpm.

3. RESULTS AND DISCUSSION

3.1. FORMULATION

Initially, the formulations prepared using HPC alone showed decreased dissolution rates in gastric fluid and pH 6.8 phosphate buffer media because of the swelling properties of HPC and the conventional circular shape of the tablets. Based on the above observations, the donut shape was designed to increase the surface area to volume ratio compared to common circular 3DP tablet shapes [41]. Though filament F1 could be printed well, its 5% drug load content was too low to develop a tablet form in use. With the same ingredients, higher drug load content filaments F2 and F3 were extruded. However, filaments F2 and F3 were too soft to be fed into the 3D printer. HPC HF and HPC EF were not selected because they had a higher viscosity than HPC LF, which confers a softer texture to the filaments. Then, HPMC K4M, a common excipient for sustained release systems, was used to increase the hardness of filaments and decrease the dissolution rate in pH 6.8 media. Thus, it came to reality that developing tablets at a drug load much greater than 5%. Eudragit® E PO is a pH-sensitive polymer that is easily dissolved at pH <5 [42], which powerfully masks the taste of ingredients because the polymer is insoluble in saliva and water. Thus, the taste-masking polymer Eudragit® E PO was used for taste masking ability of the formulations. Increasing Eudragit® E PO or the API caused the decrease of printabilities of filaments. F6 and F7 finally exhibited great printability rather than F4 or F5.

3.2. DIFFERENTIAL SCANNING CALORIMETRY (DSC)

DSC is a solid-state characterization technique, used widely for detecting thermal transitions of polymeric materials by measuring the heat required to transit phases. The DSC thermogram of CC (Fig. 2) exhibited an endothermic melting peak at around 168 °C. However, the peak was absent in the extrudates, indicating the transformation of CC from the crystalline to the amorphous state. CC dispersed into the polymers; thus, its odor and bitter taste could be masked.

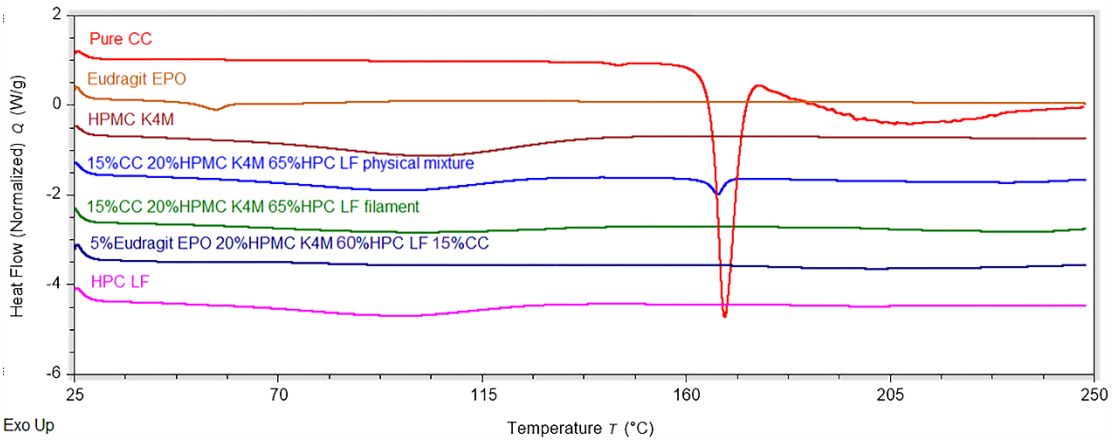

Figure 2. DSC thermogram of caffeine citrate, HPC LF, HPMC K4M, Eudragit® E PO, and formulations F6 and F7

3.3. THE REPKA-ZHANG TEST

Both softness and brittleness of the filaments affect their printability. Brittle filaments are easily crushed to fragments by gears inside the 3D printer and are difficult to feed into the 3D printer. Soft filaments are difficult to load into the 3D printer, have low abrasion resistance, usually cannot be conveyed by gears, and often block the head of the printer. The 3-point bend test is used to evaluate the breaking force, breaking distance, and breaking stress of a filament. The breaking stress is calculated from the breaking force divided by the cross-sectional area of

the filament. In this study, the filaments were extruded via a 1.5 mm diameter die, but the PLA reference used for commercial 3DP has a 1.75 mm diameter. Thus, it is meaningful to compare breaking stresses rather than breaking forces. Greater breaking stress of a filament confers a harder filament texture. Likewise, a longer breaking distance results in a softer filament. According to the relationship curve of the polymer stress against the strain, higher breaking stresses or breaking distances indicate increased brittleness. In this study, the breaking distances of filaments were greater than PLA (4.00 ± 0 mm), while the stresses were less than PLA (505.70 ± 8.74 mm). Thus, brittleness was not considered (Fig. 3).

Whether a filament is suitable for printing or not depends on the combination of the effects of stress and distance, but other factors as well. Thus, Hooke's law is used to assess the printability of filament. A 3-point bend test figure consists of two parts, one is the elastic region, which is at the very beginning of a straight line, the other is the plastic region, which is the remaining bending curve. Only in the elastic part (short bending distance) do the filaments exhibit elasticity, and when the force is removed, the filament will recover its shape. This phenomenon is similar to extending a spring. Thus, Hooke's law can be fitted. According to Hooke's law, F=-kx, “F” is the stress when the center of the filament is moved to distance “-x”. To assure the data was on the straight elastic curve, a 2 mm bending distance was chosen, and corresponding stress was obtained from the figure. The stiffness constant “k” was calculated from the known data above. If the filament has a greater “k” value, printability will be improved. F1, F6 and F7 could be printed well due to their great “k” values. On the contrary, the “k” values of other filaments (F2, F3, F4, F5) were less than 40 g/mm^3, thus, they were not printable (Table 2).

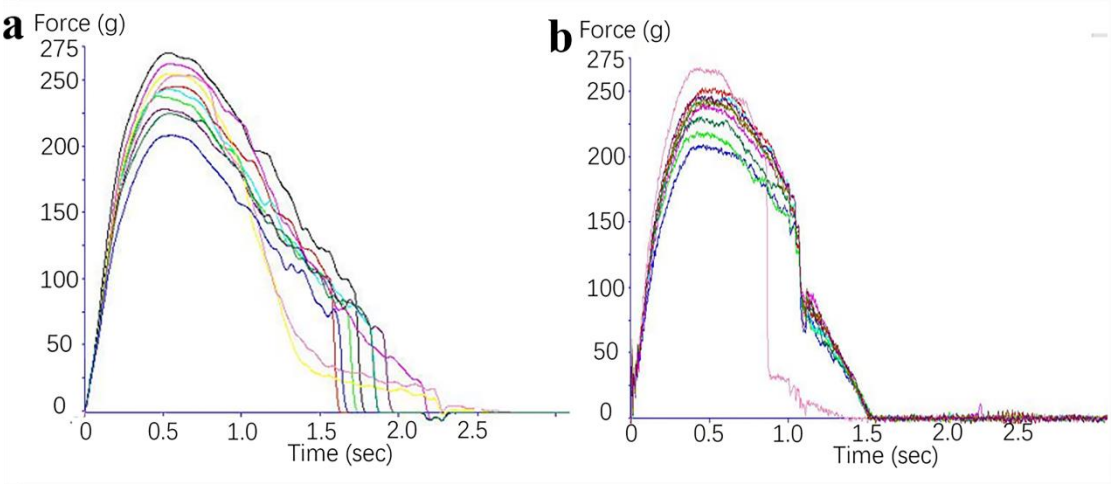

Figure 3. The force-time curve of the 3-point bend test of filaments F6 and F7. (a) F6 filaments; (b) F7 filaments.

Table 2. The 3-point bend test of filaments.

Filament	**Force(g)**	**Stress(g/mm^2)**	**Distance(mm)**	***k*(g/mm^3)**	**Printability**
F1	250.49±11.01	141.75±6.23	4.67±0.36	51.35±2.73	Yes
F6	247.60±16.94	140.11±9.59	4.62±0.21	48.30±3.52	Yes
F7	243.12±18.58	137.58±10.52	4.95±0.27	45.47±3.51	Yes
PLA	1216.35±21.02	505.70±8.74	4.00±0	151.14±4.65	Yes

∗Parameters: force (g); stress (g/mm2); distance (mm); “k” value (g/mm^3) and result of filament printability.

3.4. DIRECT COMPRESSION OF TABLETS

The physical mixture of the tablet blend had a good flowability and was compressed into 8 mm diameter circular-shaped tablets. The hardness of the directly compressed tablets was 9.82 ± 0.71 kp, while the weight was 221.29 ± 4.50 mg. The tablets were white with smooth surfaces without capping issues.

3.5. DRUG CONTENT

The drug contents of filaments and 3D printed tablets were 98–103% of the theoretical drug amounts, and there was no significant difference between the drug contents of filaments before and after 3D printing, indicating no drug degradation during 3D printing (Table 3). The temperatures of the HME and 3D printing process were 155 °C and 200 °C, respectively. However, the degradation temperature of caffeine citrate is above 250 °C, indicating that the API had good thermal stability during extrusion and 3D printing.

Table 3. Drug content of filaments and tablets of formulations F6 and F7.

Formulation		**F6 (%)**	**F7 (%)**
Filament		98.74 ± 0.28	101.63 ± 1.47
Tablet	10%	97.99 ± 0.46	100.69 ± 1.39
	50%	98.71 ± 0.43	98.60 ± 2.54
	100%	97.99 ± 0.50	99.64 ± 2.78

3.6. FOURIER TRANSFORM INFRARED SPECTROSCOPY (FTIR)

FTIR was performed to determine the post extrusion physical characterization of the extrudates (Fig. 4). Eudragit® E PO spectra showed a significant absorbance peak at 1,723 cm^{-1}, which represented C=O functional groups. The peak shifted to 1,703cm^{-1} in the F7 spectra, indicating that the carbonyl group (proton-accepting group) in Eudragit® E PO had a strong interaction with the hydroxyl group (proton-donating group) in HPC LF and HPMC K4M, inducing intermolecular hydrogen bond interactions.

From the caffeine citrate spectra, the peak at 3,471 com^{-1} corresponds to the enol O-H stretching vibrations, due to the energy increasing by HME. The peak at 1641 cm^{-1} corresponds to the amide structure (CO-NRR'). The caffeine citrate spectra showed a peak at 3,168 cm^{-1}, representing the quaternary ammonium structure composed from the tertiary amine group in

caffeine and the carboxyl group of citric acid. After the HME process, the crystal structure transformed into an amorphous form, and the two components caffeine and citric acid completely dispersed into the polymer matrix. Furthermore, the absence of the peak at 3,168cm^{-1} indicated the free tertiary amine group (proton-accepting group) did not form hydrogen bonding with the hydroxyl group (proton-donating group) in polymers, otherwise it would shift to a lower wavenumber; thus, the bitter taste of caffeine may be masked due to physical entrapment of the API in the carrier [43].

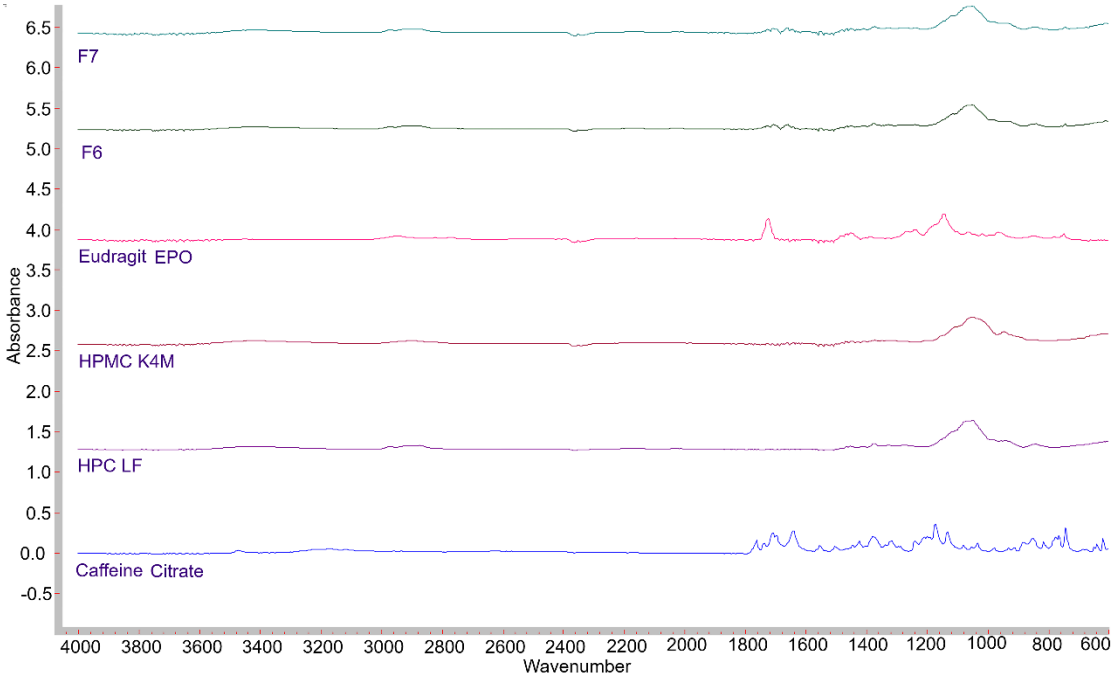

Figure 4. FTIR spectra of extrudates; F6, F7, Eudragit® E PO, HPMC K4M, HPC LF, caffeine citrate.

3.7. SCANNING ELECTRON MICROSCOPE (SEM)

SEM images of F6 printed tablets showed a significant difference between 10% infill, 50% infill, and 100% infill (Fig. 5). The surface was smooth, and the tablets showed a stepped construction, which accorded with the printing process layer on layer. The texture of 10% infill

was the most diffuse and poorly compacted, and the 100% infill was the most compact. According to the *in vitro* dissolution test data, the increased compactness resulted in a decreased dissolution rate. The tablets with a weakly compact structure readily dissolved in solution, while it took relatively more time for their counterparts with compact structures. Furthermore, a compact structure caused a harder texture of the tablets. SEM images of F6 filaments exhibited a uniform width and smooth filament surfaces as a result of the stable HME process. There was no agglomeration on the surface, suggesting a completely miscible solid dispersion system (Fig. 6). The conventional photographs of the cross-section of tablets are shown in Figure 7. SEM images of F7 printed tablets showed similar structures to the counterparts of F6 (Fig. 8), a greater infill percentage leading to a more compacted structure.

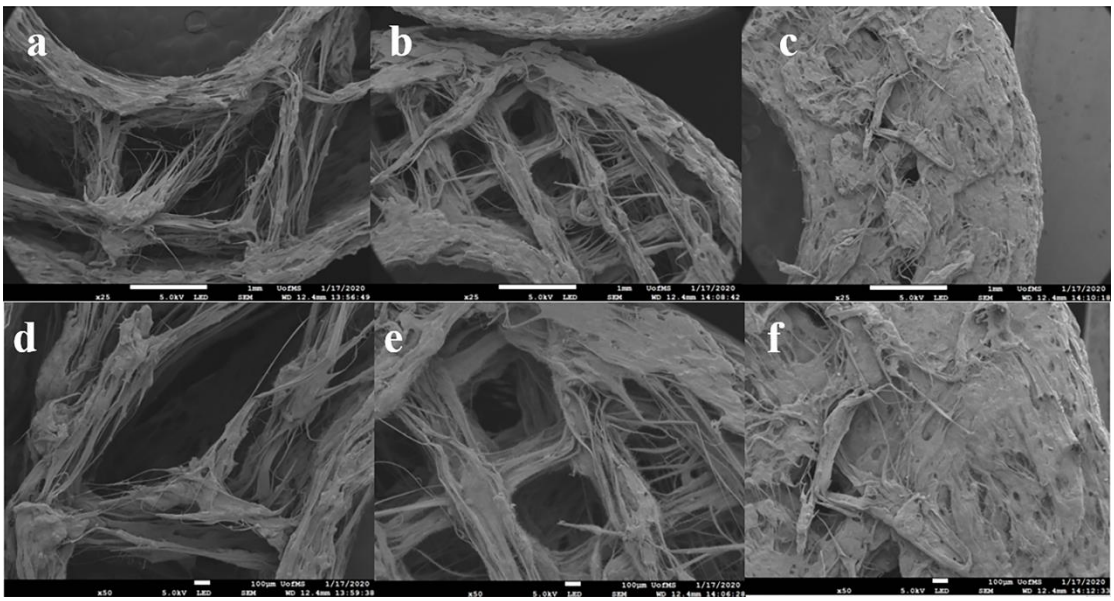

Figure 5. SEM images of the F6 cross-section at 25X and 50X magnification levels: (a) 10% infill 25X; (b) 50% infill 25X; (c) 100% infill 25X; (d) 10% infill 50X; (e) 50% infill 50X; (f) 100% infill 50X.

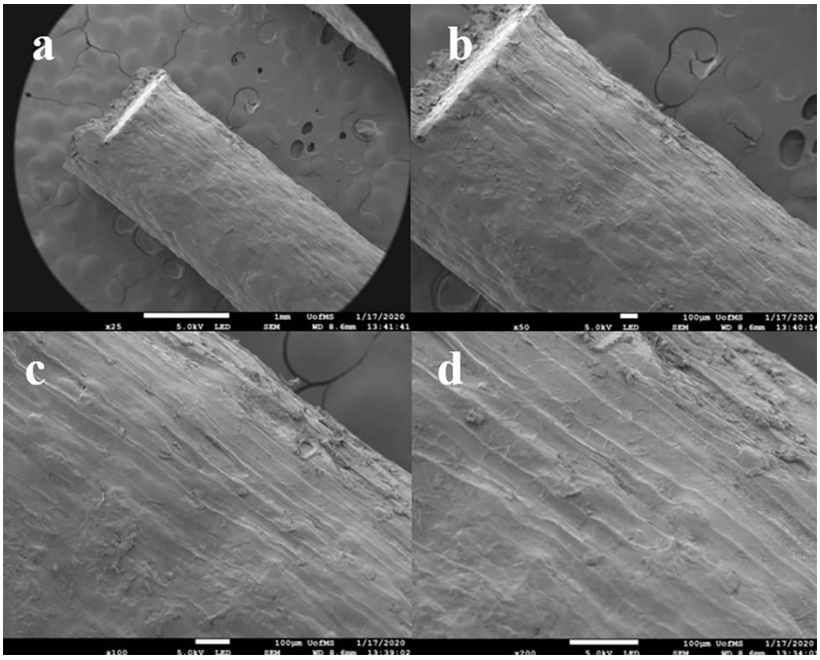

Figure 6. SEM images of F6 filaments at 25X, 50X, 100X, and 200X magnification levels: (a) 25X; (b) 50X; (c) 100X; (d) 200X.

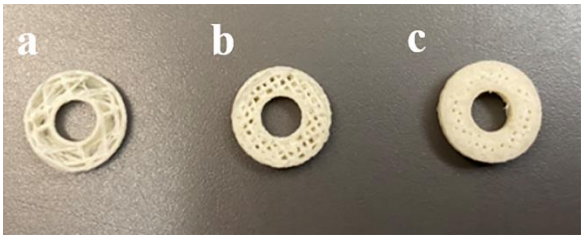

Figure 7. The conventional photographs of the cross sections of the F6 3D-printed tablets. (a) 10% infill; (b) 50% infill; (c) 100% infill.

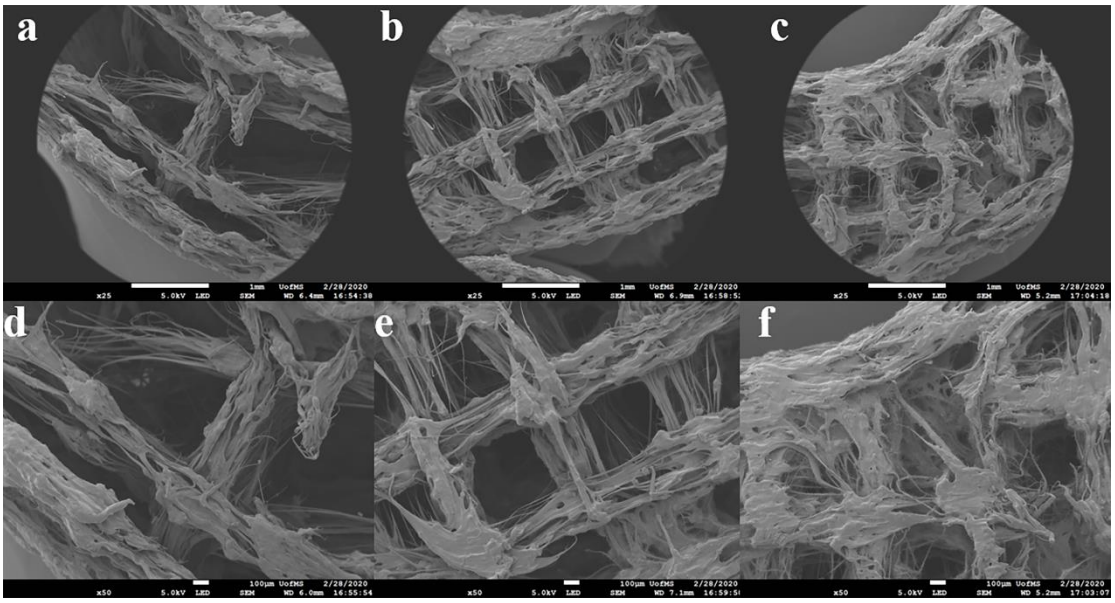

Figure 8. SEM images of the F7 cross-section at 25X and 50X magnification levels: (a) 10% infill 25X; (b) 50% infill 25X; (c) 100% infill 25X; (d) 10% infill 50X; (e) 50% infill 50X; (f) 100% infill 50X.

3.8. *IN VITRO* DRUG RELEASE STUDY

HPC LF and HPMC K4M are widely used polymers known for eroding matrix in 3D printing, so they have properties conducive to modified-release drug delivery systems. Further, the decreased drug release rate in pH 6.8 media may moderately aid in taste masking. Conversely, 3D printed tablets have a much more solid structure, decreasing the drug release rate. To attain desired drug release characteristics in 0.1 N HCl, donut-shaped 3D printed tablets with a large surface area to volume ratio compared with conventionally shaped 3DP tablets were printed, which significantly increased the drug release rate. Furthermore, the wall of the pore at the center of the tablet is not easily accessible to saliva.

Dissolution profiles of FDM 3D printed tablets with 10% infill, 50% infill, and 100% infill in 0.1 N HCl media are listed in Figure 9. As expected, for both F6 and F7 tablets, tablets

with 10% infill exhibited higher dissolution rates than the 50% and 100% infill tablets, and exhibited more than 80% drug release in 60 min. This increased dissolution rate with 10% infill density compared with 50% and 100% infill may be attributed to the increased surface area because of the pores in the tablets. The release mechanism of CC can be explained by the fact that when the hydrophilic polymers contact an aqueous solution, they may swell and become an eroding matrix, and the hydrophilic drug CC releases from the eroding matrix [44].

As shown in Figure 10, the 3D printed tablets with 10% infill exhibited higher dissolution rates than 50% infill and 100% infill. The tablets exhibited approximately 5% drug release in 60 sec and less than 10% in 120 sec. However, the concentrations of 100% infill tablets reached their maximum, because the amount of CC and the weight of the tablets were the greatest. The dissolution rate of F7 was less than that of the counterpart of F6 at the same drug infill percentage. The reason for this is that Eudragit® E PO is a pH-sensitive polymer and insoluble in the mouth but readily soluble in the stomach due to its polyacrylate molecular structure. Eudragit® E PO, owing to its adhesive properties was not suitable for 3D printing above 5% in this study. Hence, Eudragit® E PO, at 5%, exhibited improved taste-masking ability. Even the concentrations of 100% infill 3DP tablets in the first minute were less than the tasting threshold of caffeine citrate of 0.25 mg/mL [43]. Therefore, the 3D printed tablets could mask the bitter taste. Compressed tablets and pure drugs were evaluated for their drug release rates. The directly compressed tablets exhibited a 100% release in 50 sec at pH 6.8. Similarly, the pure drug exhibited a 100% dissolution rate in 30 sec. The 3D printed donut-shaped tablets released more slowly than compressed tablets and pure drugs.

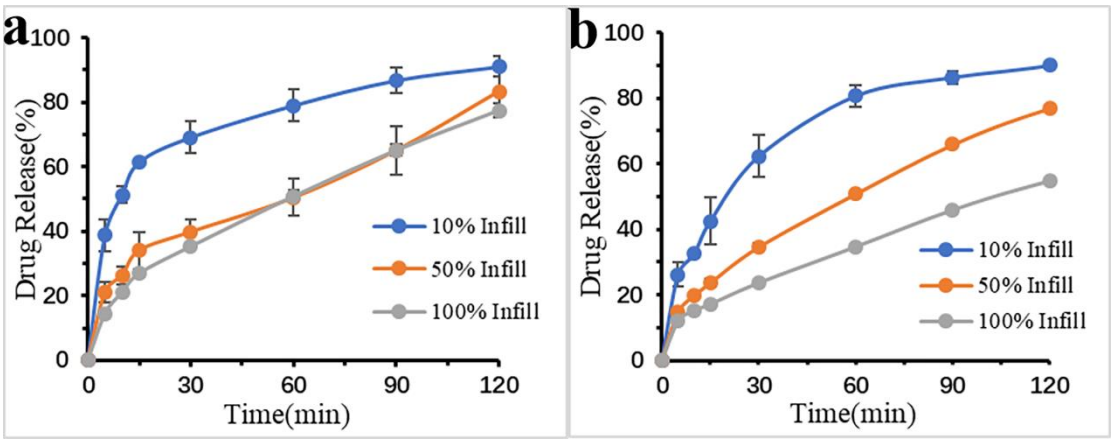

Figure 9. The dissolution profiles of 3D-printed tablets in 0.1N HCl media. (a) F6; (b) F7

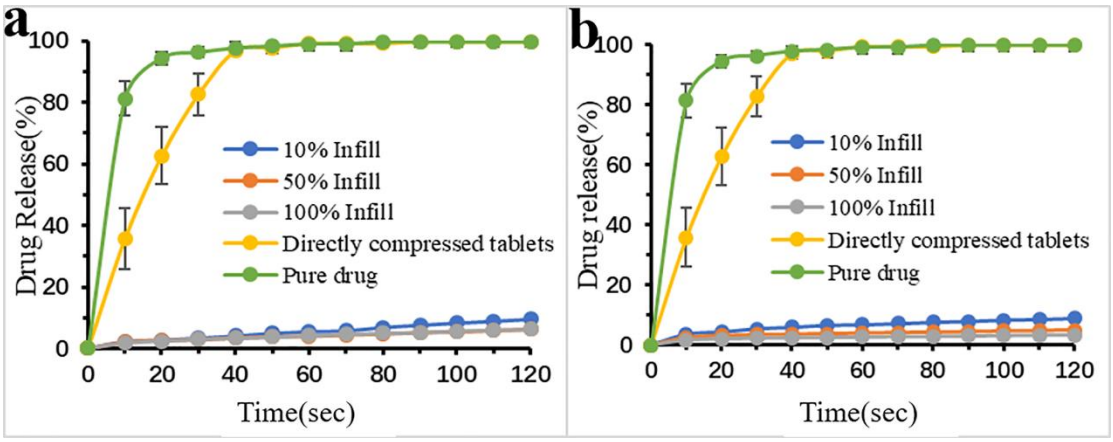

Figure 10. The dissolution profiles of 3D-printed tablets in pH 6.8 artificial saliva media (a) F6, directly compressed tablets, and pure drug; (b) F7, directly compressed tablets, and pure drug.

4. CONCLUSIONS

In this study, we successfully developed taste-masked tablets via fused deposition modeling 3D printing paired with hot-melt extrusion techniques. Three-point bend tests were performed, and the results were fitted into Hooke's law, which could explain the relationship between the data and the hardness of the filaments. The concentrations of caffeine citrate released from the 3DP donut-shaped tablets were less than the tasting threshold of caffeine citrate after 1 min, and the tablets exhibited desired drug release rates in 0.1 N HCl, indicating a taste-masking ability. The donut shape successfully modified the dissolution rates through HPC LF and HPMC K4M, leading to low dissolution rates. This study demonstrates that hot-melt extrusion has excellent potential for taste-masking, and FDM 3D printing is a new approach for manufacturing potential drug delivery systems for patient-centric pediatric populations.

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